

LITERATURE REVIEW−EFFECT OF ADDITIVES AND POST-TREATMENTS ON CORROSION RESISTANCE AND MECHANICAL PROPERTIES OF PLASMA ELECTROLYTIC OXIDATION PRODUCTS IN MAGNESIUM AND TITANIUM

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ABSTRACT

Plasma Electrolytic Oxidation (PEO) is a method of converting metal surfaces into an oxide layer with the help of plasma to improve the surface mechanical properties and corrosion resistance of metals. A PEO layer of about 10-50 μm is obtained quickly from 1 second-10 minutes at a voltage range of 150-500 V with AC or DC mode. Characteristics of the outer layer of PEO have pores and cracks, while the inner layer is relatively denser. Cracks and pores reduce the corrosion resistance and mechanical properties of the coating. In this study, a literature search was carried out on the effect of adding additives and post-treatment on the characteristics of PEO coatings grown on magnesium (Mg) and titanium (Ti) metals for biomedical applications. Mg and Ti metals have opposite chemical properties; Mg is a reactive metal, while Ti is an inert metal. Comparing the behavior of the PEO process and the coating produced by the two different metals is absorbing and necessary to understand the fundamentals of the PEO process. The results of a literature search show that the addition of additives increases the growth rate of the coating so that the coating is thicker and more wear resistant. The hardness of the coating also increases due to the additive particles trapped in the oxide layer filling the micro pores so that the surface becomes denser and more homogeneous. Therefore, corrosion resistance also increases, as indicated by a decrease in corrosion current as measured by the polarization test and an increase in the impedance modulus as measured by the electrochemical impedance test (EIS). Among the additive particles, $SiO₂$ is preferentially used as it gives significant improvement in both mechanical and corrosion properties of PEO coatings. Post treatment is necessary to seal defects in the coatings. The interesting method is alkali treatment considering its simplicity method and improvement in both corrosion resistance and bioactivity.

Keywords: Implant; post treatment; plasma electrolytic oxidation; silicon dioxide

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INTRODUCTION

The PEO coating method is an electrochemical process at high voltage that produces a ceramic oxide layer on magnesium (Mg), titanium (Ti), aluminium (Al), zirconium (Zr) and their alloys [1]. PEO has many advantages over other coating techniques, such as excellent adhesion properties of the oxide layer to the substrate, simple process, environmental friendliness and relatively low cost. Effective parameters affecting PEO coatings'

microstructural characteristics are current/voltage density, processing time, electrolyte type and composition, and temperature $[2]$. The electrolytes used in PEO can be silicates, aluminates and phosphates. The three electrolyte salts are environmentally friendly. Among the three, the phosphate electrolyte produces the predominant crystalline phase, which makes it harder and corrosion-resistant [3]. The composition of the PEO coating depends on the type of substrate and the composition of the solution used [4]. PEO coatings are expected to have biocompatibility, osseointegration with bone tissue, good corrosion resistance, and appropriate mechanical properties for biomedical applications. Generally, there are two types of implants, permanent implants and temporal (temporary) implants ^[5]. Examples of the use of permanent implants are prostheses and dental implants. While temporal implants are currently being developed using magnesium-based materials and alloys, iron, zinc, etc. Examples of the use of temporal implants are surgical staples, fixation plates in fracture repair, and stents [6].

The problems still encountered in the PEO coating are high porosity and the appearance of cracks which can reduce the mechanical properties and corrosion resistance ^[7]. Efforts can be made to optimise electrical parameters, add additives, and post-treatment of the PEO layer. The additives used for biomaterials are Ag, $CeO₂$, hydroxyapatite (HA), TiO₂, SiC, ZrO_2 , Si_3N_4 , Al_2O_3 , and SiO_2 ^[8]. Adding additives can reduce the pore size and prevent the appearance of micro-cracks^[9]. As reported by Nasiri et al., $^{[7]}$, the addition of SiC particles reduced the porosity of the PEO layer from 22.45% to 18.17%, and the hardness value increased from 280 HV to 410 HV. The coefficient of friction is lower and more stable, thereby increasing the wear resistance of the coating. The post-treatment method is another effective step that can reduce the pore diameter and cracks in the PEO layer ^[10]. This treatment can increase the corrosion resistance of the coating due to a more homogeneous surface and free of cracks. The formation of a new layer on the PEO layer after posttreatment can also trigger the ability to form new, homogeneous apatite so that bioactivity increases [11]. Therefore, this scientific review will discuss the effect of adding additives and post-treatment on the morphology and composition of the PEO layer.

METHOD

Characteristics of Magnesium and Titanium Metals

Magnesium has superior properties, including its low density $(1.35-1.85 \text{ g/cm}^3)$, strong, biocompatible, biodegradable, and non-toxic in the body $[12]-[14]$. However, Mg metal has a relatively fast degradation rate, limiting its more comprehensive application as an implant material ^[14]. The high corrosion rate causes a high rate of release of hydrogen gas and a decrease in the mechanical properties of the implant before it recovers [15], [16]. Titanium can osteogenesis $[17]$, is lighter with a density value of 1.74 g/cm³, has a high melting point of around 1660 °C, increased strength of about 210-1380 MPa, and high biocompatibility $^{[18]}$, [19]. Commercial pure titanium (CP-Ti) has a low elastic modulus value of 105 GPa close to human bone 10-30 GPa compared to alloys of Ti-6Al-4V, Co-Cr, and Stainless steel (ASTM F67) as shown in Table 1 and Table 2.

Material	Density (g/cm^3)	Elongation (GPa)	Compre-ssive strength (MPa)	toughness Fracture 1/2 (MPa.m
Natural bone	$1.8 - 2.1$	$3 - 20$	130-180	$3-6$
Mg	1.74-2.0	$41 - 45$	$65-100$	15-40
Ti	$4.4 - 4.5$	110-117	758-1117	55-115
Stainless steel	$7.9 - 8.1$	189-205	170-310	50-200
$Co-Cr$	$8.3 - 9.2$	230	450-1000	۰
Synthetic HA	3.1	73-117	600	0.7

Table 1. The physical and mechanical properties for metal implants are different compared to natural bone [5].

Metals' protective oxide layer (TiO₂) can increase stable corrosion resistance in human body fluids [13]. Implant materials in the human body must have high bioactivity and osseointegration properties. This is so that the implant can stimulate the growth of new bone tissue. In addition, implant materials must have high corrosion resistance due to being in an aggressive environment and better mechanical and wear properties [12], [20], [21].

Table 2. The physical and mechanical properties of Mg and Ti metal ^[12].

Material properties	Mg	Ti
<i>Tensile strength</i> (MPa)	152	345
Yield strength (MPa)	80	275
Melting point $(^{\circ}C)$	650	1660
Density (g/cm^3)	1,74	4,5
Thermal conductivity (W/mK)	156	16,4
Modulus elasticity (GPa)	45	105

PEO Coating Formation Mechanism

PEO is an electrochemical coating to decompose the metal surface layer into a ceramic oxide layer with the help of plasma excitation at high voltage $[12]$. The PEO layer has the characteristics of pores and micro-cracks $^{[22]}$. The PEO process can use various current source modes, including AC source, DC source, unipolar, and bipolar. Variations of the current source mode can modify the surface of the resulting PEO layer $[23]$. Usually, the voltage applied to the PEO process is between 95 V and 750 V $^{[20]}$. Electrical conditions with AC power sources produce coatings with superior quality (denser and harder) compared to DC power sources. However, there are obstacles to observing the discharge phenomenon in the PEO process with an AC power source $[24]$. In general, the schematic of the PEO process circuit can be seen in Figure 1. The substrate is placed as the anode (working electrode), which is connected to the power supply. Meanwhile, the cathode as a counter electrode uses an inert metal (platinum or graphite). Densities and current voltages commonly applied to PEO processes are in the range of 1.5 -15 A/dm² and 400-500 V for Mg alloy substrates $^{[25]}$, 6-20 A/dm² and 200-500 V for Ti alloy substrates $^{[26]}$, and 10-60 $A/dm²$ and 200-400 V for Al alloys ^[27]. Another effective parameter affecting coating is time in the range of 15-60 minutes $^{[28]}$. The electrolytes commonly used in the PEO process are phosphate, silicate, and aluminate-based electrolytes.

Figure 1. PEO process tool set schematic

The coating formation mechanism in the PEO process goes through several stages, as illustrated in Figure 2. In the first stage, a rapid increase in stress occurs, a conventional anodizing process characterized by forming a thin passive layer. During the formation of the barrier layer, the voltage increases drastically until it reaches the breakdown voltage, and leakage of the dielectric layer occurs—a small white, smooth, and homogeneous plasma splash forms on the surface at this stage. The sparks are distinct in forming the PEO layer $[24]$. In the second stage, the growth rate of the oxide film becomes reduced as the increase in stress slows down. In the third stage, the plasma spark becomes larger and turns yellow after reaching a constant voltage, and the slope becomes gentler. An orange or intense micro-discharge plasma will appear in the last stage. Voltage fluctuates with PEO processing time [29].

Figure 2. PEO layer formation mechanism

Plasma has several characteristics, including the temperature at the centre of the plasma is higher than the surrounding temperature, has a temperature between 4000-1200 K, an electron density between $1015-1018$ cm³, and the composition of the plasma consists of substances (substrate, coating and electrolyte) ^[30]. The evolution of distribution and release intensity about the processing time for PEO of magnesium alloy AZ31 in silicate electrolyte was reported by ^[31]. The longer the PEO time, the bigger and brighter the plasma will be as a measure of intensity.

Figure 3. Schematic morphology of PEO layer cross-section

Figure 3 shows the characteristics of the PEO layer, which consists of a porous outer layer, a denser inner layer, and a barrier layer. Pores are formed due to the release of gas trapped in the coating and plasma release channels during the PEO process $[12]$, $[32]$, $[33]$. The barrier layer is denser, while the inner and outer layers have pores and cracks due to solidification and thermal expansion.

Effect of Current/Voltage Density on PEO Coating Characteristics

The current density is a parameter that affects the microstructure and properties of the PEO layer. Research conducted by Zhuang et al. ^[34] explained the effect of current density on the PEO AZ31 Mg process in phosphate-based electrolytes. The current density variation applied is $5{\text -}20$ A/dm². The results of this study describe the characteristics of the microstructure, corrosion resistance, and wear resistance which are different for each variation of current density. The layer becomes thicker as the current density increases because more energy induces a reaction on the substrate surface to form a PEO layer quickly. In addition, the PEO current density also affects corrosion resistance, especially the coating formed at a current density of 10 A/dm^2 which is the most superior to other current density variations. Likewise, the wear resistance of the coating is better due to the denser layer structure. These results are similar to those reported in studies [25], [28], [35].

Table 3. Study of the effect of current/voltage density on the PEO layer

PEO, with a short time, produces a relatively homogeneous distributed layer of micropores. The pore number decreases as the coating time increases, but the pore size increases [36]. However, if the time is longer, the large pores will be filled internally because the PEO process produces micro-discharges^[37]. The layer formed on the surface results from the melting and solidification of the plasma^[38]. The pore diameter on the surface will increase with the time for oxidation ^[39]. The increase in PEO time contributes to the thickness and hardness of the coating. The PEO coating on AZ31 with current density variations of 500 A.m⁻², 700 A.m⁻², up to 900 A.m⁻² produces a coating with a hardness which is about four times greater (292-301 HV) than the substrate hardness (79 HV) $^{[28]}$. This is due to the formation of the coating's $Mg_3(PO_4)_2$ and MgO crystalline phases. However, there was an increase in the corrosion current density, and the capacitive loop diameter decreased after 15-20 minutes of PEO due to the formation of large size pores and the presence of microcracks so that the corrosive solution could easily penetrate the barrier layer. Other studies also reported similar results ^{[40], [41]}. Table 3 describes several studies that reported the effect of the current/voltage density on the PEO layer. A PEO layer of about 10-50 μm is obtained quickly between 1 second to 10 minutes of processing at a voltage range of 150-500 V.

Effect of Electrolyte Composition and Concentration on PEO Coating Characteristics

The type and concentration of electrolyte can affect the morphological properties of the PEO layer. Solutions that can be used for the PEO process on magnesium substrates include electrolytes based on silicates, aluminates, and phosphates [41], [45]-[47]. Yagi et al. [48] modified the surface of the PEO layer on the magnesium alloy ACM522 series with a phosphate-based electrolyte; the PEO layer formed consisted of a monoclinic crystalline $Mg_3(PO_4)_2$ phase. Liang et al. [49] compared the PEO process on AM50 Mg alloy in two different types of electrolytes, namely silicates and phosphates. The PEO layer with silicatebased electrolyte has finer pores and thinner thickness than phosphate-based electrolyte. The main phases for phosphate-based PEO coatings are $Mg_3(PO_4)_2$ and Mg_2SiO_4 for coatings with silicate-based electrolytes. The silicate-based PEO coating has better corrosion resistance because the coating is denser and more substantial. Similar results were reported by Li et al. ^[50] on Al alloy substrates and Yang et al. ^[50] on carbon steel substrates.

Hidayati et al. ^[51] identified a layer of PEO on top of an AZ31 Mg alloy with a phosphatebased electrolyte for 3 minutes at a current density of 400 A.m⁻², resulting in a layer with a crystalline phase of $Mg_3(PO_4)_2$ and the presence of an amorphous MgO phase and $Mg(OH)_2$. The composition of the PEO layer on the Mg alloy consists of MgO, $MgAl₂O₄$, $Mg₂SiO₄$, and $Mg_3(PO_4)_2$ depending on the type of electrolyte and type of substrate $^{[22], [36] - [38], [52], [53]}$. Aliasghari et al. ^[26] reported coating PEO on Ti substrates with a phosphate/silicate-based electrolyte. The current density is $500 \text{ mA}.\text{cm}^{-2}$, the frequency is 50 Hz , and the duty cycle is 50% for 900 seconds. The phase formed on the PEO-Ti layer consists of anatase, rutile, amorphous silica, and $Ti₂O₅$. The layer formed is about 40 to 50 µm thick with a high porosity surface. The outer layer is relatively thicker than the inner layer. Silica was detected more on the outside, and the inside was rich in titania. The current density of the titanium substrate is in the range of 300-900 mA.cm⁻².

The Effect of Additives on the Characteristics of the PEO Coating

Further research studied the effect of particles added to the PEO electrolyte on the characteristics of the oxide layer as shown in Figure 4. The deposition of microparticles on the surface of the coating has a positive impact on the wear resistance of the coating [54]. Many modifications to the PEO process have been made to increase the corrosion resistance of coatings by adding different particles in the electrolyte. The results showed an increase in the corrosion resistance and wear resistance of the PEO layer with added additives in the electrolyte. Several types of particles added to the PEO process electrolyte are GO, graphite, K_2TiF_6 , HAp, TiO₂, SiC, MoS₂, ZrO₂, Al₂O₃, CeO₂, Si₃N₄, and SiO₂^{[8], [55]–[58]}. Studies on the effect of adding additives to the PEO electrolyte on the corrosion behavior of the PEO Mg and Ti layers are presented in Table 4 and Table 5. Based on these studies it is clear that the PEO Mg and Ti processes can be carried out with different electrical parameters and additives.

Figure 4. Schematic of addition of particles in the PEO process

Table 4. Study of the effect of the addition of additives on the corrosion behaviour of the PEO Mg coating

Zhang et al., [59] have reported the effect of adding GO additive to the silicate-based PEO main electrolyte with various compositions of GO-5, GO-10, G-20, and GO-40 ml/L. The addition of additives produces a denser and more homogeneous layer. The percentage of porosity of the GO-20 additive sample decreased five times that of the sample without additives. Most of the pores on the surface of the PEO layer are filled by molten oxide from the discharge channels. The GO-40 additive sample experienced an increase in the percentage of porosity to 2.3% from the GO-20 sample (1.2%). The highest microhardness value was obtained in the GO-20 sample (572.9 $HV_{0.3kg}$) due to the denser microstructure and increased phase containing silicate. No new phase formation occurred but an increase

in the diffraction peak intensity of the main component of the PEO layer was detected with the addition of GO additives. The addition of additives encourages the formation of more MgO and $Mg₂SiO₄$ phases. There was an increase in corrosion resistance of up to three orders in the GO-20 sample with polarization resistance values increasing up to two times compared to the sample without additives. The efficiency of protection against corrosion increases due to the incorporation effect of embedded GO reducing the porosity of the PEO layer. Similar results were reported in $[60]$ with the addition of graphite additives which can increase corrosion resistance marked by a decrease in the corrosion current density of up to two orders. Graphite particles close the pores in the PEO layer so that the surface becomes more homogeneous and denser which acts as a barrier layer when in a corrosive environment.

Table 5. Study of the effect of the addition of additives on the corrosion behaviour of the PEO Ti coating

Rahmati et al. ^[61] identified the PEO layer on Mg AZ31 in a silica-based solution by adding the additive K_2TiF_6 in various concentrations. PEO coating with additives produces thicker layers with reduced pore diameter and cracks. The optimum additive concentration with the lowest porosity percentage (13.04%) was 5 g/l with a current density of 15.86 mS.cm⁻¹. As the concentration of K_2TiF_6 increases, the layer formed becomes more porous. The PEO layer without additives contains MgO, $SiO₂$ (amorphous), Mg₂SiO₄, and MgSiO₃ phases. A new phase was formed in the PEO layer by adding the additive K_2TiF_6 , namely the MgF_2 and TiO² phases (crystalline and amorphous) the greater the concentration of the additive, the more amorphous phase formation. TiO₂ fills micro pores making it denser and thickersilicate ions in the main solution form amorphous $SiO₂$, contributing to a partial sealing effect. The highest corrosion resistance was achieved with a concentration of 5 g/I K₂TiF₆ due to a dense inner layer of MgF2. The coating corrosion performance was increased, marked by the widening of the capacitive up to two loops caused by the sealing effect of the outer layer micro-pores by the incorporation of $TiO₂$ particles and the formation of $SiO₂$. Similar to that reported by ^[53] PEO Mg AZ31 with the addition of sodium tetraborate and $^{[62]}$ with the addition of K₂ZrF₆.

HAp added to a silicate-based PEO Mg AZ80 solution contributed to the growth process of the PEO layer ^[63]. The diffraction results showed the presence of HA particles in the PEO layer, so the polarization resistance value doubled with the addition of HA in the electrolyte. Self-sealing bioceramic coating with the addition of HA can increase the bioactivity properties of the coating due to its chemical and biological similarities with natural bone tissue.

Nasiri et al. ^[7] reported the research results by adding SiC nanoparticles in the electrolyte to produce a nanocomposite layer with a more stable friction coefficient than without SiC additives. Yu et al. [1] reported PEO on Mg AZ31 in silicate and phosphate-based electrolytes with SiC nanoparticles (~100–2000 nm) after dilution to prevent particle agglomeration during the PEO process. This study showed an increase in the growth rate of the coating without and with the addition of SiC nanoparticles, from 21 µm/minute to 37 µm/minute. In addition, corrosion resistance increases based on a decrease in the current density of corrosion from $2x10^{-6}$ A.cm⁻² to $9.25x10^{-7}$ A.cm⁻². The wear resistance of the coating is closely related to the surface hardness. SiC is a very hard particle (3000 HV) distributed on the oxide layer's surface ^[1]. Nano-sized ceramic particles trapped in the coating are protective in increasing wear resistance. In addition, the addition of SiC nanoparticle additives in the electrolyte increases the hardness value of the coating compared to no additives with the same process parameters. SiC nanoparticles fill the pores or are trapped in the oxide layer, increasing the hardness value of the layer [64].

The addition of additives in the PEO electrolyte also affects the corrosion behaviour of the coating. The effect of SiC nanoparticles incorporated in the pores is a barrier to the transfer of corrosive Cl ions and suppresses the corrosion current density ^[64]. The low electrical conductivity of SiC nanoparticles acts as a barrier in electron transfer. The amount of Mg is the most dominant compared to other elements, especially element C which comes from SiC nanoparticles. The same thing was also observed in the research of Mohedano et al. [65]. The PEO process with phosphate-based electrolyte on Mg AM50 resulted in a decrease in pore size and density on the surface by increasing the concentration of additive particles from 2 g/l to 10 g/ l (ZrO_2 , α -Al₂O₃, and CeO₂). A better additive added in the formation of PEO coating is CeO2, with long-term corrosion performance. Adding additives to the PEO solution can increase the hardness value of the PEO layer, as shown in Figure 5.

Figure 5. Effect of additive on the hardness value of the PEO Mg coating [7], [8], [60], [64], [66].

The PEO process on Ti grade 2 was reported by Malinovschi et al. [67] using a DC source of 0.36 A.cm⁻² and electrolyte NaAlO₂ with various concentrations from 10-20 g/l. The dominant crystalline phases formed were α -Al₂O₃ and γ-Al₂O₃. Other phases with minor concentrations are $TiAl₂O₅$ and $Na₂T₄O₉$. The increase in electrolyte concentration and the length of time for oxidation increased the thickness of the PEO layer. The thickest layer has better wear resistance. In addition, the addition of electrolyte concentration can also reduce the size of the micropores formed on the surface of the coating, thereby increasing corrosion resistance. Sarbishei et al. [68] also reported PEO results on Ti substrates in silicate-based electrolytes added to alumina nanoparticles. Alumina particles were found to precipitate to fill the pores on the surface of the PEO results, thereby reducing the amount of porosity (15.2%). The PEO coating can increase titanium's corrosion resistance by up to 10 times. These results are similar to the study by Vasilyeva et al. ^[69]; the coating surface becomes more homogeneous after adding acetonitrile to the primary electrolyte and increases adhesion to the substrate.

SiO² is widely chosen as an additive in PEO electrolytes because it produces a functional, corrosion-resistant, wear-resistant coating and has good biodegradability ^[75]. Based on the analysis results in Table 6, it can be confirmed that the optimum concentration of $SiO₂$ particles to increase corrosion behaviour is up to two orders of magnitude in magnesium alloys, namely in the range of 2 g/l to 5 g/l $^{[76]}$.

Table 6. Study of the effect of adding $SiO₂$ additives on the morphology and corrosion behavior of PEO coating

PEO Coating Post Treatment Method

Several methods that have been widely used as alternatives to improve the properties of PEO coatings include hydrothermal [80], sealing treatments (sol-gel, alkali treatment, organic and inorganic coatings) [10], [81]–[87], silane layer [81], [88]–[90], and conversion surface treatment [86], [91] .

Tian et al. [80] reported PEO Mg AZ31 in a silicate-based electrolyte by hydrothermal (HT) method as post-treatment. The HT solutions used were 0.1 M Ca-EDTA, KH₂PO₄, and 1 M NaOH. The HA layer formed on top of the PEO layer managed to cover the pores on the surface, thereby increasing the corrosion resistance in the SBF solution based on the PDP test results. The PEO layer has a corrosion potential value that shifts to a relatively negative position (E_{corr} = -1.640 V). In contrast, the value of the corrosion current density decreases significantly (i_{corr} = 4.74x10⁻⁷ A.cm⁻²) about two orders compared to the substrate (E_{corr} = -1.508 V, i_{corr}= $1.4x10^{-5}$ A.cm⁻²). The PEO-HT coating presented a more positive corrosion potential (Ecorr = −1.234 V) and a much lower corrosion current density (i_{corr} = 2.1x10⁻⁹ A.cm⁻²), about four times the substrates. PEO/HT coating also has good bioactivity and, biocompatibility, flexible fabrication. It is suitable for adhesion and proliferation, making it promising in surface modification of biodegradable magnesium-based implants for orthopaedic applications.

The sealing treatment method was reported by Van Phuong et al. ^[10], with sealing results in two different solutions (cerium and phosphate) on the PEO Mg layer. PEO electrolyte

composition consisted of 0.7 M NaOH, 0.1 M NaF, 0.1 M Na₃PO₄ and 0.1 M Na₂SiO₃ for 5 minutes. The first sealing treatment was in a 0.023 M Ce(NO₃)₆H₂O solution and 0.25 M H2O at 25ºC. Second sealing in 0.1 M NaH2PO⁴ solution at 90ºC. Both were carried out for 20 minutes each. The results of this treatment succeeded in closing the pores and reducing cracks in the PEO layer. The first sealing treatment stored the cerium compound in the PEO layer, but some of the layers would dissolve if soaked longer. The combination of double sealing can significantly increase the corrosion resistance of the PEO coating. After the first sealing treatment and a second sealing in a phosphate solution, it can change CeO into a more stable CePO₄.

The results of a similar study were reported by Mingo et al. [81], identifying the characteristics of the PEO Mg AZ91 layer by the post-treatment sealing method in three different solutions (serum, stained, and ODP acid). Compounds formed after sealing consists of CeO2, MgSn $(OH)_{6}$, and SnO. Even though this treatment did not completely cover the surface of the PEO layer, it still filled in the pores and cracks, thereby slightly increasing the corrosion resistance. Sealing in ODP acid solution gave the best results due to the increased hydrophobicity of the ODP monolayer.

The sol-gel hybrid method and epoxy coating were reported by Liu et al. [85] on the PEO Mg AM50 coating, which was adequate for closing pores and free from cracks. This is due to an organic/inorganic composite layer which can increase the adhesion strength, corrosion resistance, and wear performance. Fluorine-containing polymers are hydrophobic on the surface of the coating. The epoxy resin distributes the corrosion inhibitor into the pores of the PEO coating. The thickness of the coating will increase with increasing immersion time, although the surface roughness will decrease. These results are similar to those reported by [92], [93] .

Alkali treatment is a treatment that can fill the pores of the PEO layer without destroying the bioactivity properties of the layer. In general, this method is used to improve the characteristics of PEO coatings on Mg and Ti alloys so that they can contribute to implant applications. Research reported ^[94] alkaline treatment using 0.25 M NaOH solution at 80° C for 90 minutes confirmed the presence of a layer of Mg (OH)₂. The sub-microns in the PEO layer can form homogeneous apatite, making it practical for increasing the corrosion resistance and bioactivity of AZ31 alloy. ^[11] they have also presented the results of an alkaline treatment study with a 3 M NaOH solution at 60˚C for 1 hour on silicate-based PEO Mg. The total Ca/P ratio increased due to the formation of a thick corrosion layer and covered the pores of the PEO layer after the alkali treatment. This step can effectively reduce the pore size and increase the surface homogeneity of PEO Mg layers with spherical or globular morphology. This treatment can increase corrosion resistance, as evidenced by a decrease in the value of the corrosion current density from 1.7×10^{-6} A.cm⁻² to 4.42×10^{-7} A.cm⁻². In addition, the alkaline treatment is also a simple treatment compared to plasma spray and sputtering, does not involve high temperatures, and can increase the surface homogeneity of the PEO layer.

CONCLUSION

Based on the results of the literature review, it can be concluded that the process and characteristics of the PEO coating on Mg and Ti are enjoyable to discuss because Mg and Ti have opposite properties, namely Mg is a reactive metal, while Ti is an inert metal. Both metals are used in biomedical implant applications. The problem researchers are still facing with PEO Mg and Ti is irregular cracks and pores, which reduce the coatings' corrosion

resistance and mechanical properties. PEO, adding additives, produces a coating with better corrosion and wear resistance. The additive that can potentially be used in the PEO process for biomedical implant applications is $SiO₂$ because it produces a PEO layer with good wear resistance and is biodegradable. The optimum concentration of $SiO₂$ particles to increase the corrosion behaviour of the PEO coating is in the range of 2 g/l to 5 g/l. Alkali treatment methods can increase the corrosion resistance of the PEO coating and improve the bioactivity properties of the coating for biomedical applications.

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